

## Enhancement of US-CT registration accuracy for spinal surgery


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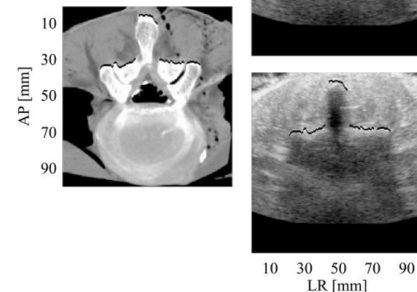
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Project proposal – Advanced Computer-Integrated Surgery (601.656)

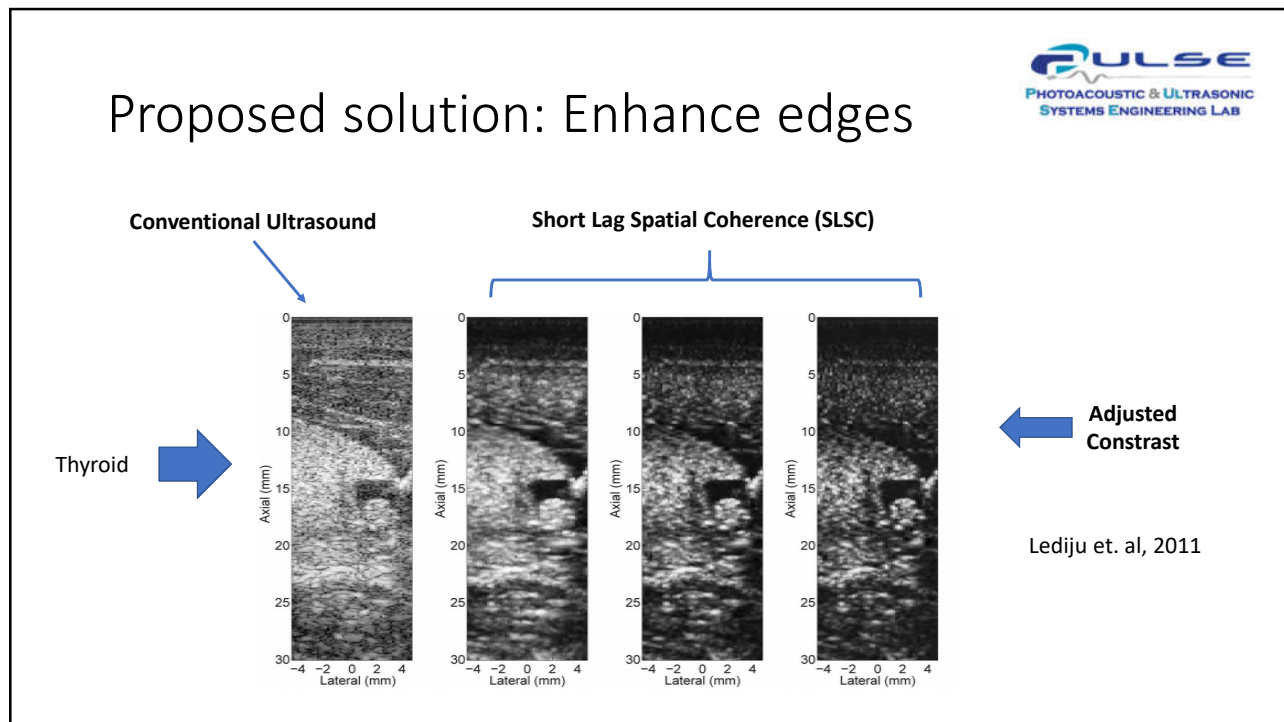
Spring 2018


## Background / Challenge

1. Preoperative plan  Intraoperative situation
2. **Ultrasound Imaging (US)**
  - ✓ **Good intraoperative imaging technique : low cost and simplicity of use**
  - ✗ **Poor signal-to-noise ratio (SNR)**  
Reflection from tissues with high acoustic impedance
  - ✗ **Deformed imaged** due to physician pressure
3. **US/CT registration**
  - **Intensity-based registration** (MRI applied in brain/ CT applied in kidney )
  - **Feature extraction (Sobel gradient)**
  - **Multi-component similarity measurement**



Brendel et. al, 2002





## Objective

Explore methods to improve accuracy of US-CT image registration through improved US image resolution

**Specific Aims:**

1. Enhance bony features in US images to improve resolution for automatic registration
2. Develop a robust beamformer to improve the appearance of bone in US images
3. Explore registration improvement when considering additional information from Photoacoustic (PA) images

# Technical Approach

**Conventional beamforming: Delay and Sum (DAS)**

$$\tau(x_1, x, z) = (z + \sqrt{z^2 + (x - x_1)^2}) / c,$$

$$s(x, z) = \int_{x-a}^{x+a} RF(x_1, \tau(x_1, x, z)) dx_1.$$

**Advanced beamforming: Short lag spatial coherence (SLSC)**

$$\hat{R}(m) = \frac{1}{N - m} \sum_{i=1}^{N-m} \frac{\sum_{n=n_1}^{n_2} s_i(n) s_{i+m}(n)}{\sqrt{\sum_{n=n_1}^{n_2} s_i^2(n) \sum_{n=n_1}^{n_2} s_{i+m}^2(n)}}$$

$$R_{sl} = \int_1^M \hat{R}(m) dm \approx \sum_{m=1}^M \hat{R}(m).$$

Feature extraction

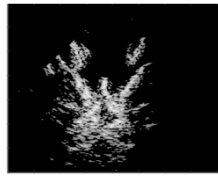


Fuzzy C-means segmentation

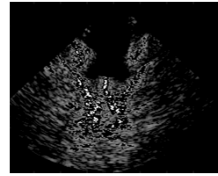
- Bone (desired region)
- Water (and undesired reflections)
- Regions outside imaging boundaries (for phased arrays)



US image



Bone (desired region)



Water



Regions outside

# Technical Approach

Control the quality of US image

- Dynamic range of log compression for DAS
- Cumulative summed lag value for SLSC
- Regularization parameter for robust SLSC

Registration



Mattes Mutual Information

Evaluation



Mean Square Error (MSE)

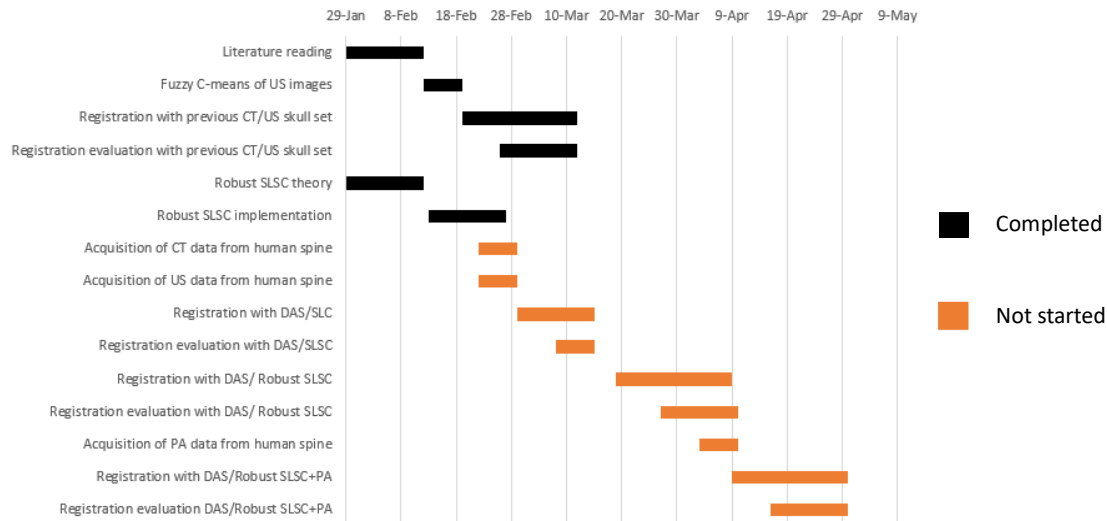
## Deliverables

Minimum (March 8 <sup>th</sup> )	Expected (April 5 <sup>th</sup> )	Maximum (April 19 <sup>th</sup> )
<b>Images:</b> Automatic registration of SLSC/DAS US images to CT images of spine specimen (hard tissue)	<b>Images:</b> add robust SLSC to registration framework	<b>Images:</b> add PA to registration framework
<b>Equation:</b> Propose algorithm for a robust SLSC technique		
<b>Graph:</b> Show registration performance when varying quality parameters for SLSC and DAS	<b>Graph:</b> add quality parameters for robust SLSC (e.g., kernel size and regularization parameters)	<b>Graph:</b> compare CT-PA and CT-US registration performance using PA images

## Dependencies

- Acquisition of CT images of human spine
  - Scheduling use of CT machine options:
    - Medical campus (Professor Siewerdsen and his postdoc)
    - Homewood campus (Michelle Graham, CAMP Lab Members)
  - Cannot acquire CT myself because did not take the CT training course
- Calibration phantom to validate registration methods (ground truth)
- Availability of the spine sample
  - Coordinate with Blackberrie Eddins

## Work plan



## Bibliography



- Roche et al. **“Rigid Registration of 3-D Ultrasound With MR Images: A New Approach Combining Intensity and Gradient Information”**, 2001
- Wein et al. **“Simulation and Fully Automatic Multimodal Registration of Medical Ultrasound”**, 2007
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- Wong et al. **“Real-time ultrasound-guided spinal anesthesia using the SonixGPS needle tracking system: a case report”**, 2013
- Shubert et al. **“A novel drill design for photoacoustic guided surgeries”**, 2017