

# Photoacoustic Registration and Visualization: Project Plan

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Group 9

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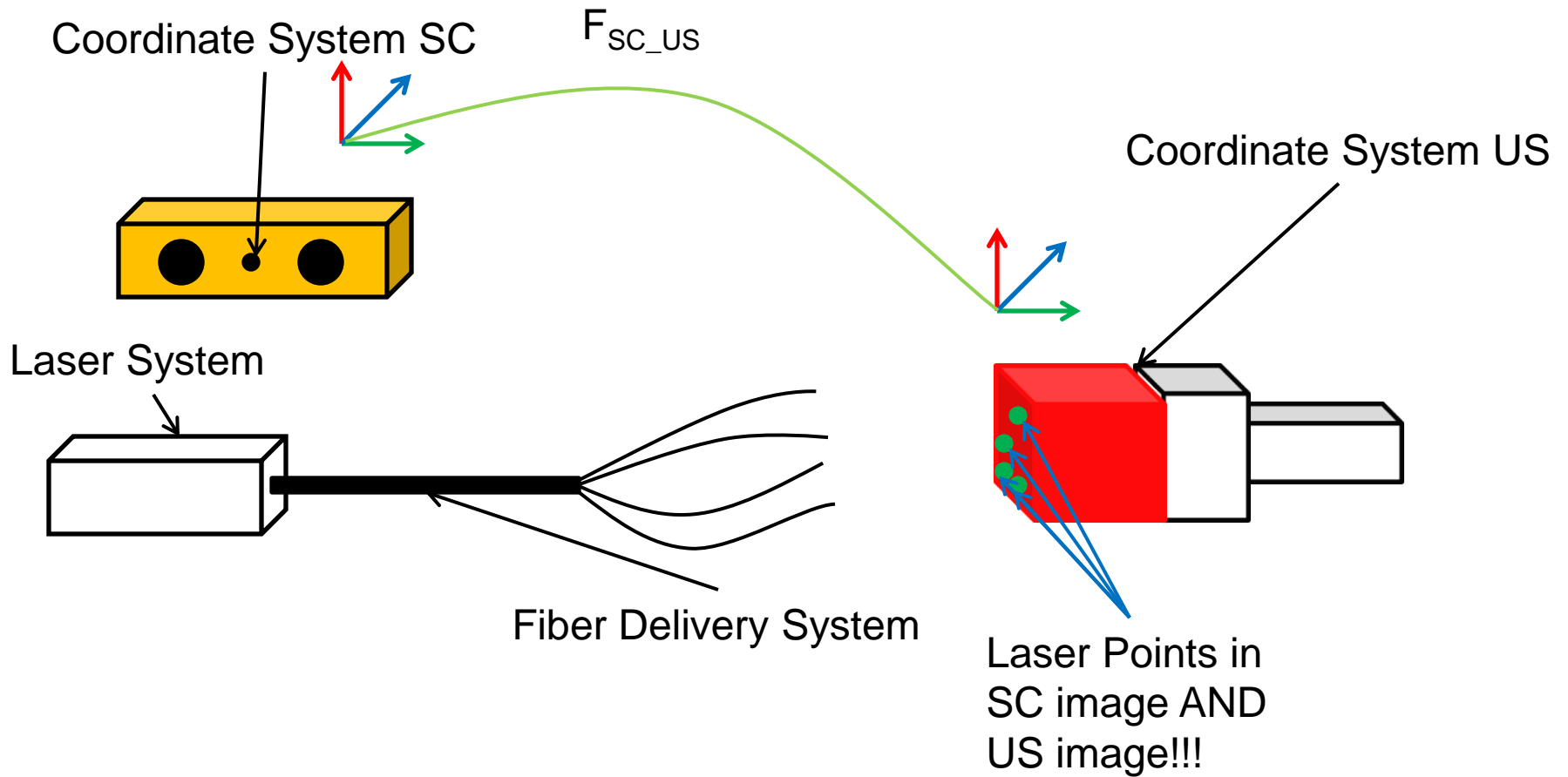
# Overview

- Summary
- Background
- Motivation
- Workflow
- Technical Approach
- Deliverables
- Dependencies
- Milestones
- Management Plan
- Reading List

# Summary

- Goal: Demonstrate automatic registration between 3D Stereocamera space and 3D Ultrasound space using Photoacoustic imaging in a system with visualization
- Team Member: Alexis Cheng
- Mentors: Emad Boctor, Russell Taylor, Jin Kang

# Summary



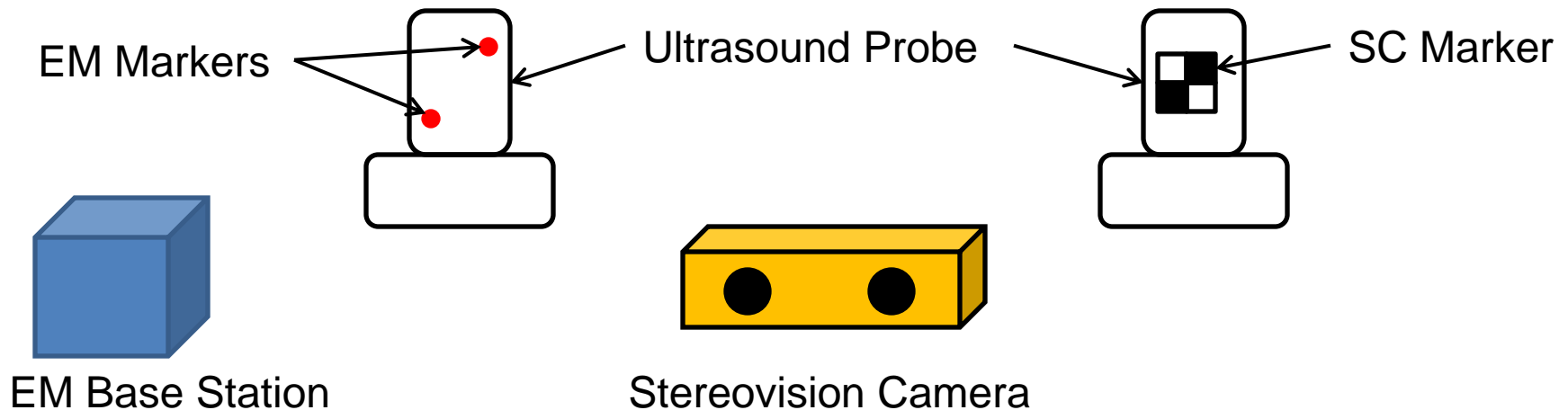
# Background

- Photoacoustic Imaging
  - Discovered in 1880 by Alexander Graham Bell
  - Light Waves are absorbed by the material, causing thermal excitation
  - Thermal excitation causes Acoustic wave
  - Acoustic waves can be detected with an Ultrasound probe

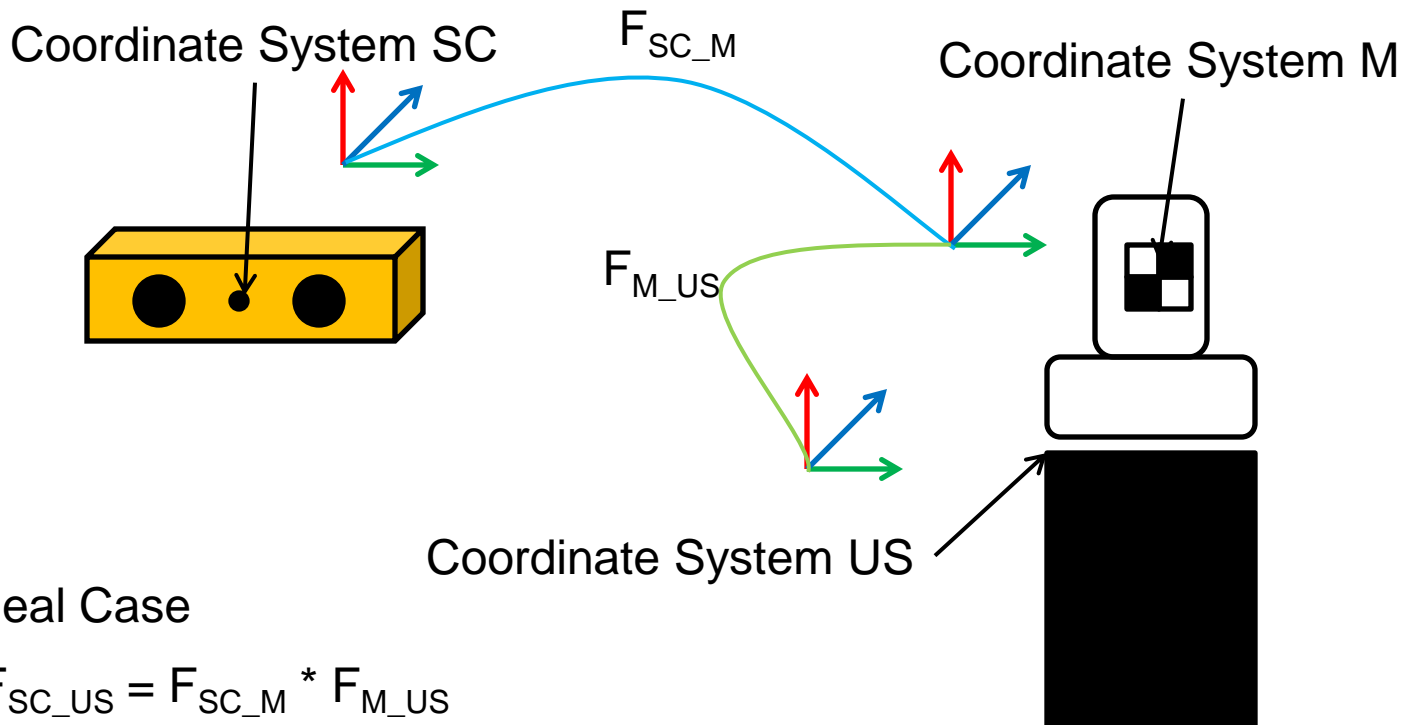


# Motivation

- Surgical Tracking Systems are widely used in Computer Assisted Interventions
- Common Tracking Systems include Electromagnetic and Stereo Camera



# Motivation



Ideal Case

$$F_{SC\_US} = F_{SC\_M} * F_{M\_US}$$

Real Case with Errors

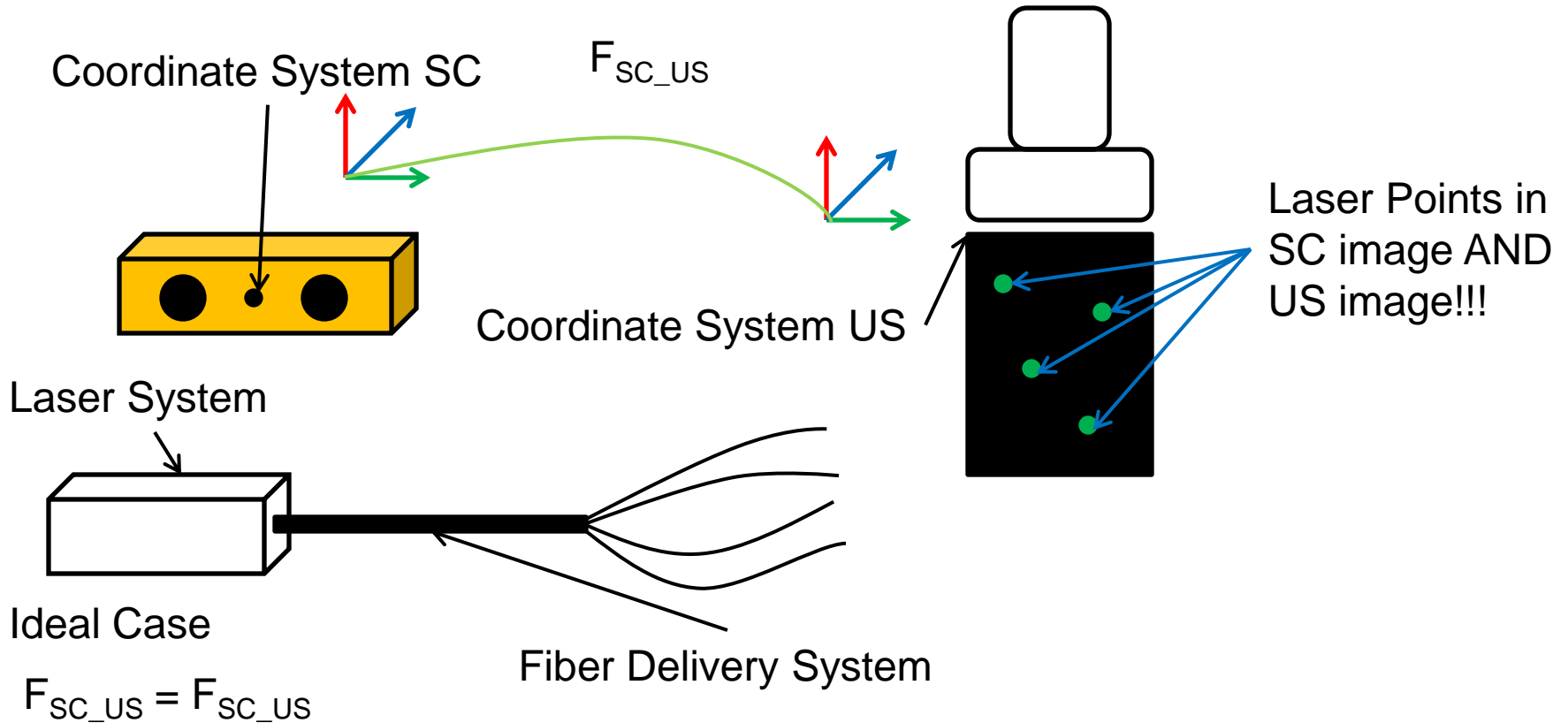
$$F_{SC\_US} * \Delta F_{SC\_US} = F_{SC\_M} * \Delta F_{SC\_M} * F_{M\_US} * \Delta F_{M\_US}$$

# Motivation

- $\Delta F_{SC\_M} = [I + sk(a_{SC\_M}), e_{SC\_M}]$
- $\Delta F_{M\_US} = [I + sk(a_{M\_US}), e_{M\_US}]$
- $\Delta F_{SC\_US} = [I + sk(a_{SC\_US}), e_{SC\_US}]$
- [2]  $a_{M\_US} = 3.26$  degree,  $e_{M\_US} = 3.08$  mm
- [3][4]  $a_{SC\_M} = 0.11$  degree,  $e_{SC\_M} = 0.5$  mm
- 90% Confidence Intervals
- $a_{SC\_US} = R_{M\_US} * a_{SC\_M} + a_{M\_US}, a_{SC\_US} \leq 3.37$  degree
- $e_{SC\_US} = e_{SC\_M} - R_{SC\_M} * sk(p_{M\_US}) * a_{SC\_M} + R_{SC\_M} * e_{M\_US}, e_{SC\_US} \leq 3.58$  mm



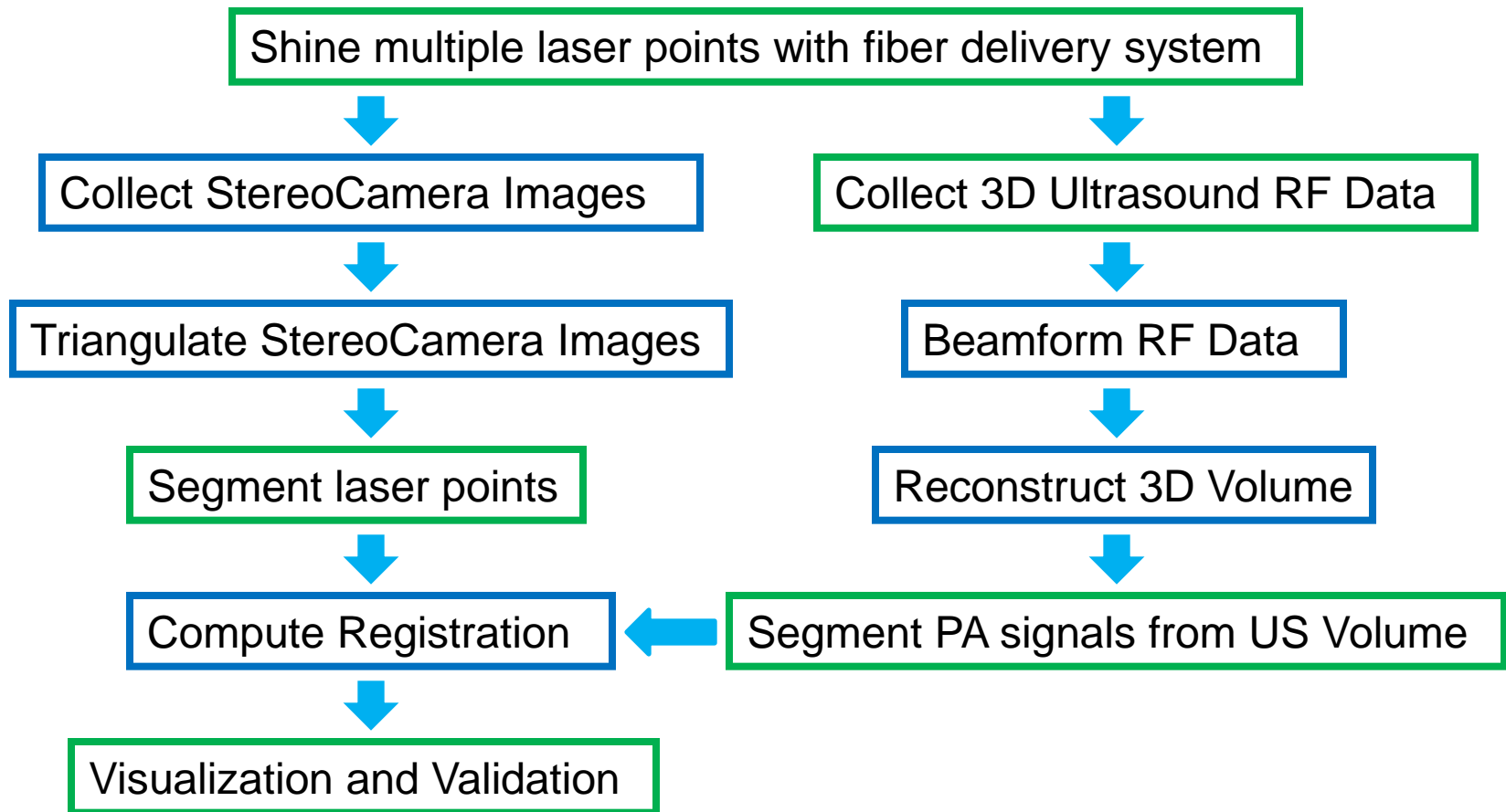
# Motivation



Real Case with Errors

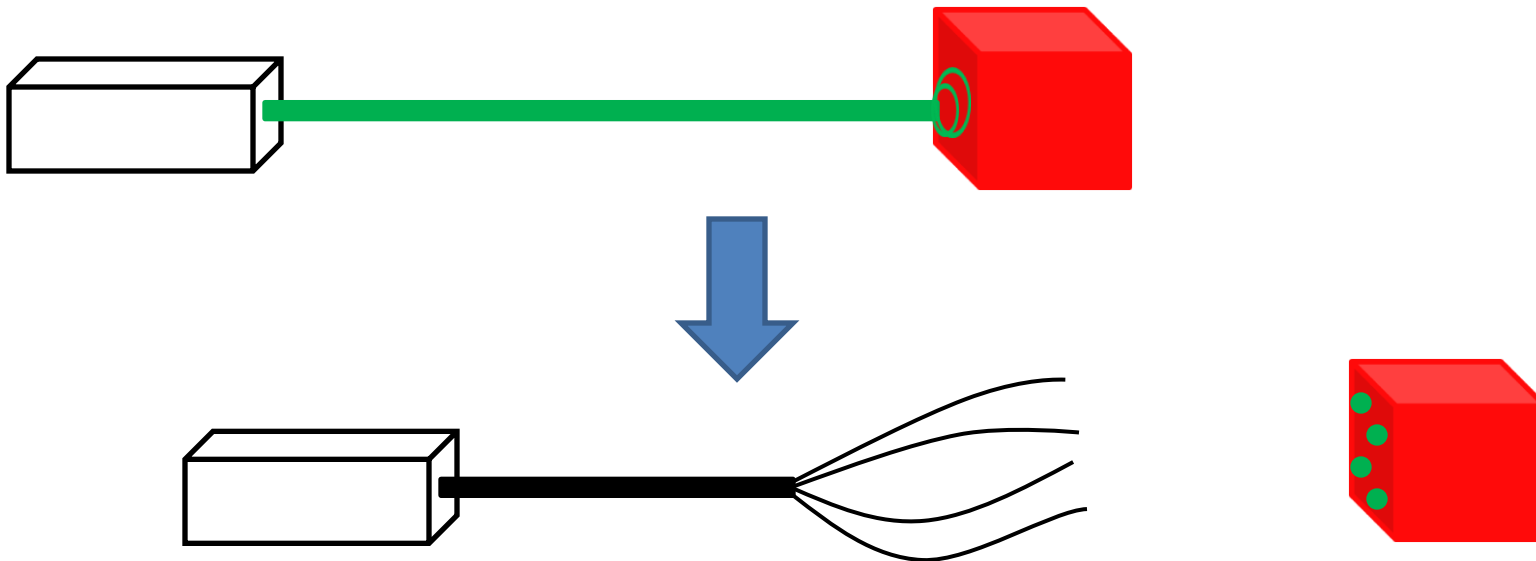
$$F_{SC\_US} * \Delta F_{SC\_US} = F_{SC\_US} * \Delta F_{SC\_US}$$

# Workflow



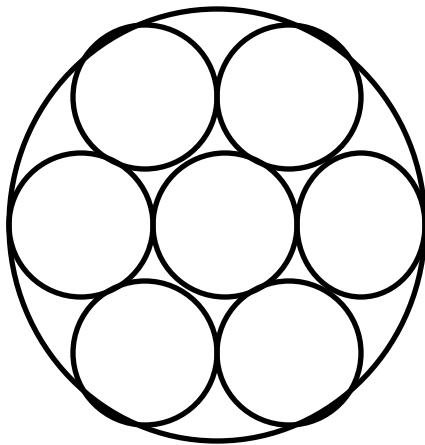
# Technical Approach (1)

- From sequential single point firing to multi-point firing
  - Develop fiber delivery system



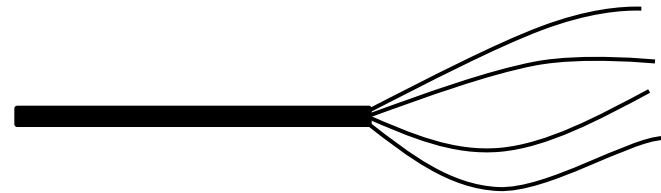
# Technical Approach (1)

Fiber Bundle



Laser Light IN

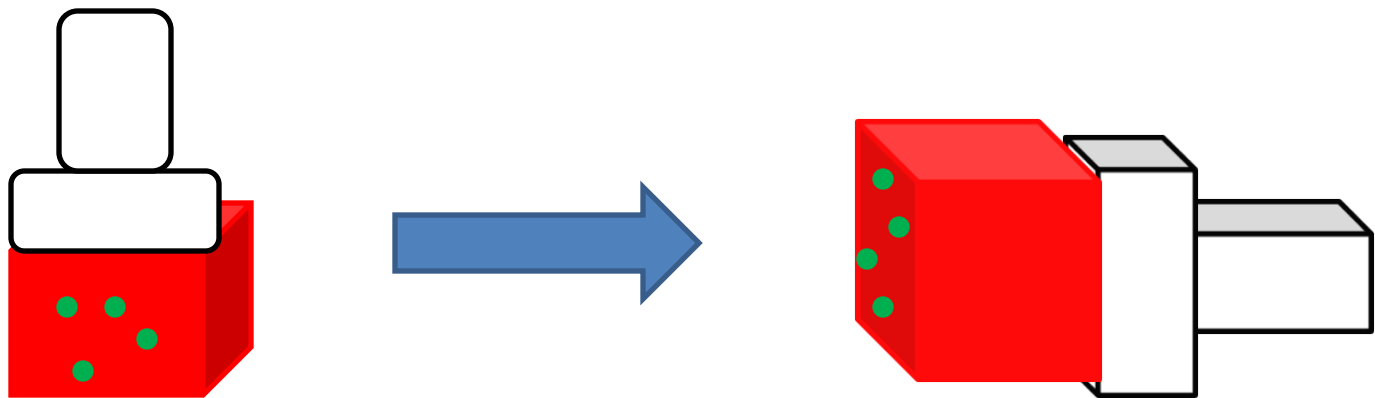
Split Bundle at end



Laser Light OUT

# Technical Approach (2)

- From 2D Ultrasound to 3D Ultrasound
  - Previous Issues
    - Required accurate placement of ultrasound probe to receive superficial acoustic waves



# Technical Approach (2)

- Use existing 2D RF acquisition software



# Technical Approach (3)

- From Manual Segmentation to Automatic Segmentation
  - Previous Issues
    - Results could not be reliably recalculated from data
    - Cumbersome to find intensity thresholds with trial and error
    - Inability to extend to real-time

# Technical Approach (3)

StereoCamera Images

Use color to make images binary



Determine points based on characteristics of each high intensity region

Ultrasound Volume

Determine intensity threshold based on intensity histogram



Use threshold to make volume binary



Determine points based on characteristics of each high intensity region



# Technical Approach (4)

- Arun's Method [1]

$$\bar{\mathbf{a}} = \frac{1}{N} \sum_{i=1}^N \tilde{\mathbf{a}}_i$$

$$\tilde{\mathbf{a}}_i = \mathbf{a}_i - \bar{\mathbf{a}}$$

$$\bar{\mathbf{b}} = \frac{1}{N} \sum_{i=1}^N \tilde{\mathbf{b}}_i$$

$$\tilde{\mathbf{b}}_i = \mathbf{b}_i - \bar{\mathbf{b}}$$

$$\mathbf{H} = \sum_i \begin{bmatrix} \tilde{a}_{i,x} \tilde{b}_{i,x} & \tilde{a}_{i,x} \tilde{b}_{i,y} & \tilde{a}_{i,x} \tilde{b}_{i,z} \\ \tilde{a}_{i,y} \tilde{b}_{i,x} & \tilde{a}_{i,y} \tilde{b}_{i,y} & \tilde{a}_{i,y} \tilde{b}_{i,z} \\ \tilde{a}_{i,z} \tilde{b}_{i,x} & \tilde{a}_{i,z} \tilde{b}_{i,y} & \tilde{a}_{i,z} \tilde{b}_{i,z} \end{bmatrix}$$

$$H = U * S * V^t$$

$$R = V * U^t$$

$$T = \tilde{\mathbf{b}} - R * \tilde{\mathbf{a}}$$

$$F = [R, T]$$

# Technical Approach (5)

- Validation of calculated Transformations
  - Visualization of Ultrasound points in Camera Space
- Given that  $SC_k = F_{SC\_US} * US_k$  for k points
  - Target registration error (TRE) of points not used in registration
    - $TRE = SC_{test} - F_{SC\_US} * US_{test}$
    - Where  $F_{SC\_US}$  is computed with k-1 points

# Technical Approach (5)

- Given that  $SC_k = F_{SC\_US} * US_k$  for k points
  - Fiducial registration error (FRE) of points used in registration
    - $FRE = SC_k - F_{SC\_US} * US_k$  for all k
    - Where  $F_{SC\_US}$  is computed with k points
  - Fiducial localization error (FLE) of points used in registration
    - $FLE = SC_k - TRUE SC_k$  for all k
    - $FLE = US_k - TRUE US_k$  for all k

# Deliverables

- Minimum
  - Phantom and Ex-vivo Experimental Results with 3D Ultrasound
  - Ability to project multiple laser points concurrently
  - Visualization only shows points overlaid together
  - Automatic Segmentation working on 2D Ultrasound images or each individual 3D Ultrasound slice

# Deliverables

- Expected
  - Minimum Deliverables
  - Visualization overlays points and representation of 3D Ultrasound volume
  - Automatic Segmentation working on 3D Ultrasound volume

# Deliverables

- Maximum
  - Expected Deliverables
  - Ability to collect 3D RF data without manually actuating motor
  - Complete system integrated together

# Dependencies

- Access to Laboratories
  - Dr. Kang's Lab
    - Have access to key already
  - Dr. Boctor's Lab area
    - Have access to pass code already
- Access to Equipment
  - Laser and Optics
    - Have access to Dr. Kang's lab already
  - Ultrasound Machine
    - Have access to Dr. Boctor's Lab area already
- Access to Phantom materials
  - Have access to Dr. Boctor's lab area already

# Milestones

- Phantom Construction
  - Date: February 27
  - Criteria: Create phantom suitable for 3D PA imaging
- 3D Ultrasound
  - Date: February 27
  - Criteria: Be able to manually segment the PA signal from a 3D volume



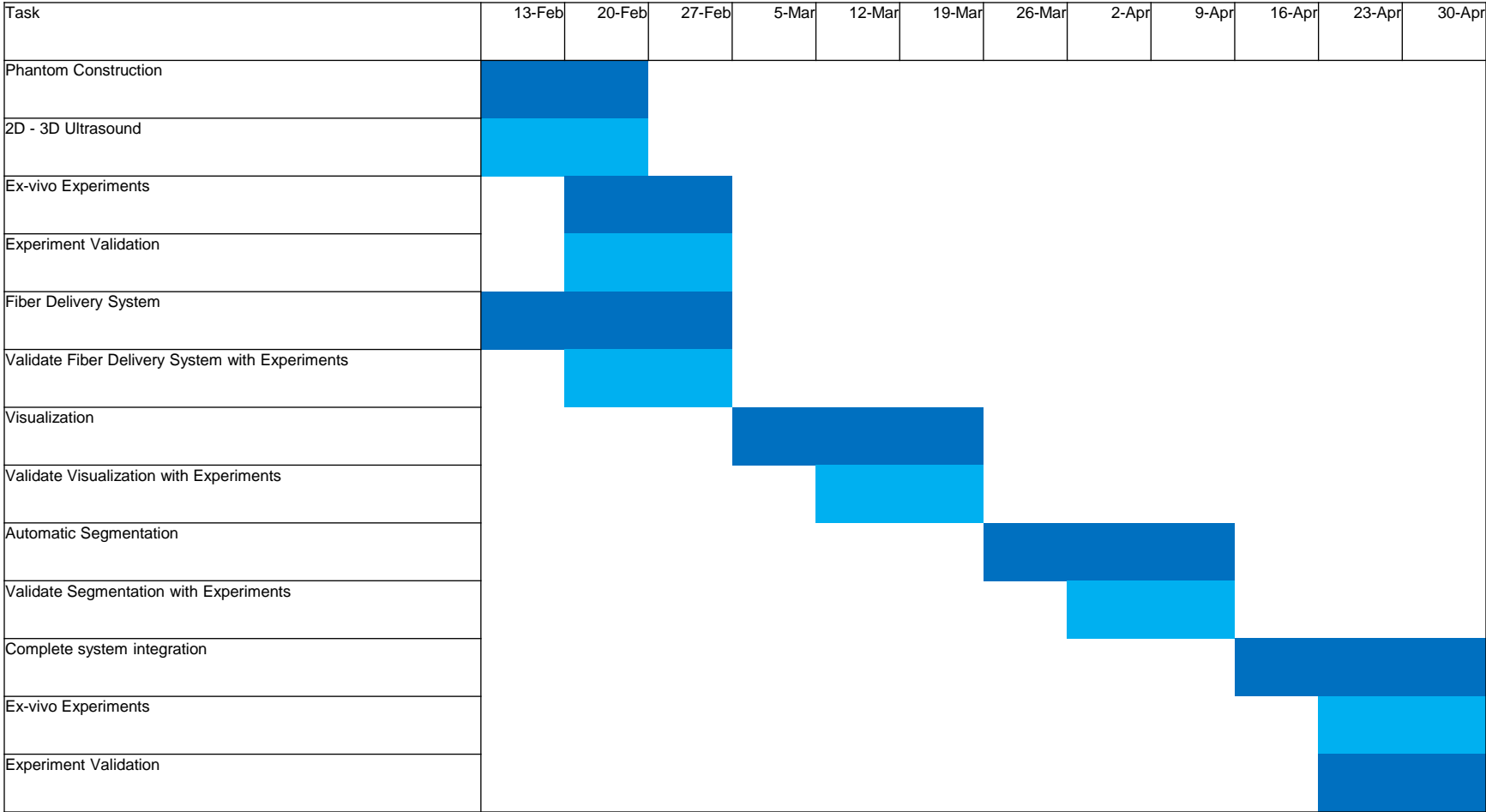
# Milestones

- Fiber Delivery System
  - Date: March 5
  - Criteria: Develop a fiber that can shine multiple laser spots at once
- Visualization
  - Date: March 26
  - Criteria: Be able to display SC and US points in the SC space

# Milestones

- Automatic Segmentation
  - Date: April 16
  - Criteria: Able to segment desired PA signal from a set of images
- System Integration
  - Date: May 7
  - Criteria: Pieces fit together

# Milestones



# Management Plan

- Schedule weekly meetings with mentors
- Review timeline and milestones weekly
- Adjust timeline accordingly weekly

# Reading List

- Hoelen C. et al. “Three-dimensional photoacoustic imaging of blood vessels in tissue”. Optics Letters 1998. Vol. 23-8:648-650
- Kuo N. et al. “Photoacoustic imaging of prostate brachytherapy seeds in ex vivo prostate”. SPIE 2011
- Oberhammer P. et al. “Optimization and Quantification for Rigid Point Based Registration for Computer Aided Surgery”. Advances in Medical Engineering 2007. Vol. 114-3:230-235
- Pham D. et al., “Current Methods in Medical Image Segmentation”. Annual Review of Biomedical Engineering 2000. Vol. 2:315-337
- Vyas S. et al., “Intraoperative Ultrasound to Stereocamera Registration using Interventional Photoacoustic Imaging”. SPIE 2012
- Xu M. et al. “Photoacoustic Imaging in Biomedicine. Review of Scientific Instruments”. Review of Scientific Instruments 2006, 77

# Future Work

- Low power high frequency laser diodes
  - Replace expensive laser!
- Pre-operative Model Registration with Fiducials
- Move to DaVinci System
- Tool tracking
- Sub-surface imaging

# References

- [1] Arun K. et al., “Least-Squares Fitting of Two 3-D Point Sets”. IEEE PAMI, 9-5:698-700, September 1987.
- [2] Boctor E. et al., “A Novel Closed Form Solution for Ultrasound”. ISBI 2004
- [3] Navab N. et al., “Camera-Augmented Mobile C-Arm (CAMC) Application: 3D Reconstruction using Low Cost Mobile C-Arm”. MICCAI 1999, 688-697
- [4] Wiles A. et al., “Accuracy assessment and interpretation for optical tracking systems”. Medical Imaging 2004, vol. 5367: 421-432

# Questions?