



Shoulder and Elbow Joint Angle Tracking With Inertial Sensors

El-Gohary, M., & McNames, J. (2012). Shoulder and elbow joint angle tracking with inertial sensors. IEEE Transactions on Biomedical Engineering, 59(9), 2635–2641. https://doi.org/10.1109/TBME.2012.2208750

Team 14 Guanhao(Dean) Fu Mentors: Peter Kazanzides, Ehsan Azimi

Statement of project



https://github.com/qian256/ur5_unity





Summary of problem & key results

Problem:

• Continuously estimate the angles of human shoulder and elbow using 2 IMUs

Key Results:

- Computed joint angles using inertial sensor (IMU)
- Validation joint angles using optical tracker





Significance of key result

• Good agreement between inertial tracker and optical tracker for both regular and fast-speed

movement of the arm.

- Average correlation coefficient r > 0.95
- RMS angle error < 6.5 deg
- Peak error < 9.8 deg

TABLE II Average Correlation r, RMSE, and Peak-to-Peak Error Between Optical and Inertial Angles of Shoulder and Elbow

Task	r	RMSE(°)	Peak Error(°)
Elbow Flexion/Extension	0.98	6.5	9.8
Forearm Supination/Pronation	0.95	5.5	7.8
Shoulder Flexion/Extension	0.98	5.5	7.9
Shoulder Abduction/Adduction	0.99	4.4	8.1

[4]: El-Gohary, et al., 2012





Why this paper?

Paper

- Measures shoulder and elbow joint angles using 2 IMUs
- Validates computed joint angles with optical tracker

CIS 2 Project

- Measures shoulder and elbow joint angles using 2 IMUs
- Validates computed joint angles in Unity with

virtual robot arm





Background – IMU

- Low cost MEMS* systems
- 3-axis Gyroscope angular velocity
- 3-axis Accelerometer linear acceleration
- 3-axis Magnetometer magnetic field strength
- Internal sensor fusion: gyro + acc + mag / gyro + acc
- Sensor fusion output: 3DOF orientation in body fixed frame of

the IMU (Euler angles/Quaternions)

*: microelectromechanical





https://lp-research.com/wp-content/uploads/2020/ 03/20200310LpmsB2HardwareManual.pdf



Background – Human Arm Joint Angles



Joint	DOF
Shoulder	3
Elbow	2
Wrist	2

[5]: D. Naidu, et al., 2011





Background – DH Parameters



[1]: https://robotacademy.net.au/lesson/denavit-hartenberg-notation/

$$A_i = Rot_{z,\theta_i} Trans_{z,d_i} Trans_{x,a_i} Rot_{x,\alpha_i}$$

4 "Basic" transformation parameters

- rotate around the zj-1 axis by an angle θi
- translate along zj-1 axis by a distance di
- translate along the new x axis by a distance aj
- rotate around the new x axis by an angle αj

[2]:http://www.aeromech.usyd.edu.au/MTRX4700/Course_Documents/ material/lectures/L2_Kinematics_Dynamics_2013.pdf





Paper – Human Arm Kinematics



[4]: El-Gohary, et al., 2012

DENAVIT-HARTENBERG PARAMETERS FOR THE ARM MODEL

Frame	α_{i-1}	a_{i-1}	d_i	θ_i
1	0	0	0	θ_1
2	$\pi/2$	0	0	$\theta_2 + \pi/2$
3	$\pi/2$	0	l_{u}	$\theta_3 + \pi/2$
4	$\pi/2$	0	0	$\theta_4 + \pi/2$
5	$-\pi/2$	0	$l_{\rm f}$	θ_5

For shoulder joint:

"When a joint has n-DOFs, it can be modeled as n joints of one DOF connected with n – 1 links of zero length" - El-Gohary, et al., 2012





Paper – Experimental setup



Fig. 2. Reflective markers and Opal inertial sensors (APDM, Inc.) placement on the arm of one of the subjects.

[4]: El-Gohary, et al., 2012





Paper – Kalman Filter

State estimation x(Observation

 $x(n+1) = f_n [x(n), u(n)]$ $y(n) = h_n [x(n), v(n)]$

State estimation

$$\begin{aligned} \theta_i(n+1) &= \theta_i(n) + T_{\rm s}\dot{\theta}_i(n) + \frac{1}{2}T_{\rm s}^2\ddot{\theta}_i(n) \\ \dot{\theta}_i(n+1) &= \dot{\theta}_i(n) + T_{\rm s}\ddot{\theta}_i(n) \\ \ddot{\theta}_i(n+1) &= \alpha\ddot{\theta}_i(n) + u_{\ddot{\theta}_i}(n) \end{aligned}$$

where $i = \{1, \ldots, 5\}$ of the five angles, $\theta_i(n)$ is the *i*th angle at time n, $\dot{\theta}_i$ is the angular velocity, $\ddot{\theta}_i$ is the angular acceleration, $u_{\ddot{\theta}_i}(n)$ is a white noise process with zero mean, α is a process model parameter, and $T_s = 1/f_s$ is the sampling period.

KF output: posterior estimate (after measurement correction) of the five joint angles

Observation

$$\begin{split} \dot{\omega}_{z} &= \dot{\theta}_{3} + \dot{\theta}_{1}s\theta_{2} \\ \dot{\omega}_{x} &= \dot{\theta}_{1}c\theta_{2}s\theta_{3} - \dot{\theta}_{2}c\theta_{3} \\ \dot{\omega}_{y} &= \dot{\theta}_{1}c\theta_{2}c\theta_{3} + \dot{\theta}_{2}s\theta_{3} \\ \dot{\omega}_{y} &= \dot{\theta}_{1}c\theta_{2}c\theta_{3} + \dot{\theta}_{2}s\theta_{3} \\ \dot{\omega}_{x} &= -l_{u}[\dot{\theta}_{1}^{2}c\theta_{2}^{2} + \dot{\theta}_{2}^{2}] - gc\theta_{1}c\theta_{2} \\ \dot{v}_{x} &= -l_{u}[\dot{\theta}_{1}^{2}c\theta_{2}^{2} + \dot{\theta}_{2}^{2}] - gc\theta_{1}c\theta_{2} \\ \dot{v}_{y} &= l_{u}[c\theta_{2}s\theta_{2}s\theta_{3}\dot{\theta}_{1}^{2} - 2\dot{\theta}_{2}c\theta_{3}s\theta_{2}\dot{\theta}_{1} + \ddot{\theta}_{2}s\theta_{3} + \ddot{\theta}_{1}c\theta_{2}c\theta_{3}] \\ &+ g[c\theta_{3}s\theta_{1} + c\theta_{1}s\theta_{2}s\theta_{3}] \\ \dot{v}_{z} &= l_{u}[c\theta_{2}c\theta_{3}s\theta_{2}\dot{\theta}_{1}^{2} + 2\dot{\theta}_{2}s\theta_{2}s\theta_{3}\dot{\theta}_{1} + \ddot{\theta}_{2}c\theta_{3} - \ddot{\theta}_{1}c\theta_{2}s\theta_{3}] \\ &- g[s\theta_{1}s\theta_{3} + c\theta_{1}c\theta_{3}s\theta_{2}] \end{split}$$

ω: angular velocity from gyroscopev-dot: linear acceleration from accelerometer



Paper – Results



Fig. 5. Shoulder abduction/adduction angle estimates by the optical system (dashed line) compared to inertial angles estimate (solid line), and the error in gray.



Fig. 6. Shoulder flexion/extension estimates by the optical system (dashed line) compared to inertial angles estimate (solid line), and the error in gray.

Result of shoulder angles - abduction/adduction, and flexion/extension





Paper – Results



Fig. 4. Forearm supination/pronation estimates by the optical system (dashed line) compared to inertial angles estimate (solid line), and the error in gray.



Fig. 7. Elbow flexion/extension during fast arm movement. Inertial estimates (solid line) compared to estimates from the optical system (dashed line).

Result of forearm angles - forearm supination/pronation, and elbow flexion/extension





Assessment

Pros

- Detailed Kalman Filter model
- High correlation between inertial(post-KF) output and optical tracker output
- Longer assessment period than other IMU based work (2-min)

Cons

- No Shoulder internal/external rotation validation data and did not explain why
- Did not explain why IMU's integrated KF is not sufficient, given their sensor are ~\$4k a piece





Relevance to project

- Real-time joint angle tracking, and generalized to track any limb movement
- Assumption is the same: the trunk of the human subject must remain perpendicular to the ground
- Sensor placement is a good starting point for CIS 2 project
- Further study potential: does the IMU drift in Z-axis really affect human-in-the-loop operation such as teleoperation surgery? (comparison between IMU internal KF and subject specific KF)





Conclusion

- Useful theory of arm D-H parameter
- Solid summary of other relevant inertial tracking work
- Application specific yet generalized enough for other limb tracking
- Very relevant to CIS 2 project





Reference

- 1. D-H https://robotacademy.net.au/lesson/denavit-hartenberg-notation/
- 2. D-H <u>http://www.aeromech.usyd.edu.au/MTRX4700/Course_Documents/material/lectures/L2_Kinematics_Dynamics_2013.pdf</u>
- 3. IMU https://stanford.edu/class/ee267/lectures/lecture9.pdf
- 4. El-Gohary, M., & McNames, J. (2012). Shoulder and elbow joint angle tracking with inertial sensors. IEEE Transactions on Biomedical Engineering, 59(9), 2635–2641. <u>https://doi.org/10.1109/TBME.2012.2208750</u>
- Naidu, D., Stopforth, R., Bright, G., & Davrajh, S. (2011). A 7 DOF exoskeleton arm: Shoulder, elbow, wrist and hand mechanism for assistance to upper limb disabled individuals. IEEE AFRICON Conference, (September), 1–6. https://doi.org/10.1109/AFRCON.2011.6072065





Backup: Statement of project

- Design a wearable system that
 - Captures surgeon's arm motion in 4DOF at tool (palm)
 - Can control state-of-the-art robot such as UR3 or dVRK use Unity for virtual demo
 - Has high precision in position control of the slave robot
 - Has a similar workspace as the Da Vinci's MTM
 - Has a way to recognize surgeon's intention to engage/disengage with the system (rules of engagement)



